

# Naked eye evaluation and quantitative detection of the sugarcane leaf scald pathogen, *Xanthomonas albilineans*, in sugarcane xylem sap

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**Abstract.** Sugarcane leaf scald caused by the bacterium *Xanthomonas albilineans* is a major disease of sugarcane worldwide. Whereas erratic symptoms make phenotypic detection challenging, molecular methods require expensive instruments and labour, and longer sample-to-answer times. We report a novel method for detection of *X. albilineans* DNA in sugarcane xylem sap. The method involves (i) boiling lysis-based DNA extraction from sugarcane sap; (ii) magnetic purification of target sequences directly from the lysate through use of magnetic bead-bound capture probes; and (iii) DNA sandwich hybridisation platform for HRP/TMB/H<sub>2</sub>O<sub>2</sub> reaction-based naked eye visualisation and electrochemical detection of the target. The method is sensitive (limit of detection 100 fM) and reproducible (relative standard deviation <7%) with linear dynamic range 100 fM–1 nM ( $R^2 = 0.99$ ). The method was tested on a range of sugarcane cultivars of known resistance ratings (susceptible, intermediate resistant, and resistant) for leaf scald disease from an inoculated field trial. Detection levels agreed with the resistance rating of cultivars tested. In addition, qPCR results strongly correlated with our assay ( $r = 0.91$ – $0.99$ ,  $P < 0.01$ ) and cultivar resistance rating. We believe that our assay could be useful for rapid screening as well as sensitive quantification of target pathogen DNA in infected sugarcane plants.

**Keywords:** leaf scald disease, *Xanthomonas albilineans* detection, naked eye evaluation of leaf scald disease, electrochemical detection of leaf scald disease, sugarcane xylem sap.

Received 22 October 2020, accepted 10 March 2021, published online 26 May 2021

## Introduction

Plant pathogens are among the major threats to sugarcane productivity and biodiversity. Lost production and measures to control pests and diseases cost hundreds of millions of dollars every year (McLeod *et al.* 1999). Leaf scald is a major sugarcane disease caused by a xylem-inhabiting bacterium *Xanthomonas albilineans* (Ashby) Dowson (Garces *et al.* 2014). The disease has been reported in more than 60 countries; however, Australia, USA, Philippines, Vietnam and Thailand are among the most affected countries (Rott and Davis 2000). Leaf scald was first recorded in Australia in 1911 and its occurrence has since been reported in all sugarcane growing regions (Rott and Davis 1995; Davis *et al.* 1997). Leaf scald can cause severe yield loss or total destruction of crops if susceptible varieties are planted (Hoy 1994). Comstock *et al.* (1997) estimated a yield loss of

19.5–32% in Florida, and Rott (1995) reported a yield loss of 12–21% in Guadeloupe, France. Besides reductions in yield and harvestable stalk number, leaf scald can also reduce fibre quality and sucrose contents and affects the juice quality (Rott *et al.* 1997). Elimination of high yielding varieties in cultivar selection programs is an indirect but significant loss incurred by leaf scald. It has been reported that, in Australia, ~20% of potentially high yielding varieties are rejected because of leaf scald susceptibility (Birch 2001). The national plant biosecurity status report has identified leaf scald as a high priority pest threat (Plant Health Australia 2019).

Narrow chlorotic (white) stripes or patches of chlorotic tissue on sugarcane leaves are characteristic leaf scald symptoms. *X. albilineans* produces a highly potent pathotoxin, called albicidin, which is mainly responsible for

these foliar symptoms (Birch and Patil 1985). Albicidin is a DNA gyrase inhibitor and blocks replication of chloroplast DNA, which ultimately leads to the inhibition of chloroplast differentiation and appearance of chlorotic symptoms on infected leaves (Cociancich *et al.* 2015). Albicidin also plays a key role in systemic invasion and possibly unpredictable transition from latency to active disease. Although albicidin-deficient mutant *X. albilineans* strains are able to colonise sugarcane efficiently, transgenic sugarcane varieties expressing the albicidin detoxification gene *albD* show resistance to leaf scald (Birch *et al.* 2000). Thus, albicidin is considered necessary for development of leaf scald.

Plants infected with *X. albilineans* may show two forms of symptoms, chronic and acute, and two distinct phases, latent and eclipse (Birch and Patil 1985; Rott and Davis 2000). Each of these pathogenic manifestations poses particular challenges in terms of disease diagnosis and control. The acute form, which often appears subsequent to a rainy period followed by a prolonged dry weather (Rott and Davis 1995), leads to abrupt wilting of plants resulting in death, leaving little room for preventive interventions (Rott and Davis 2000). During the latency phase, plants may remain asymptomatic for months or years before environmental conditions are favourable for the disease to trigger an outbreak (Ricaud and Ryan 1989). On the other hand, during the eclipse phase, a plant can appear diseased or healthy depending on when it is inspected because characteristic white lines on leaves continue to appear and disappear throughout the eclipse phase (Rott and Davis 1995). Many sugarcane cultivars can tolerate the pathogen without exhibiting symptoms, or the symptoms may escape detection because the disease expression may be too insignificant to be recognised (Ricaud and Ryan 1989; Rott and Davis 1995; Rott *et al.* 1997). Disease diagnosis as well as assessment of sugarcane test cultivars for leaf scald resistance is generally based on observation of the phenotypic symptoms. Thus, not only do latency and erratic nature of symptom expression make disease diagnosis challenging, but susceptible cultivars may also be assigned false 'resistant' ratings. Difficulty in accurately identifying infected plants has contributed to the worldwide spread of leaf scald via apparently 'healthy' planting materials (Rott 1995). As alternatives to symptom-based diagnosis, various other approaches such as isolation on selective media (Davis *et al.* 1994), ELISA (Comstock and Irely 1992), end-point PCR (Pan *et al.* 1999) and qPCR (Garces *et al.* 2014) have been employed for leaf scald diagnosis. However, these methods are not without shortcomings. Isolation on selective media, though very efficient especially for detecting *X. albilineans* in symptomless plants, is cumbersome and time-consuming (Wang *et al.* 1999). Immunological and molecular methods are robust and sensitive but require a centralised laboratory setup. High initial investment is required to set up laboratory infrastructure, and reliance on skilled labour significantly increases the costs of operation. In most of the cases, the testing site is located far from the disease-affected areas, therefore additional measures and costs for processing, storage and transport of samples from the field to laboratories are also involved. And last, there is a significant time lapse between sample collection and communication of the results back to farmers.

In recent years, electrochemical biosensors have emerged as potential contenders for the development of rapid, cost-efficient and amplification-free DNA/RNA detection platforms (Shiddiky *et al.* 2007, 2010; Boriachek *et al.* 2018). Although tremendous progress has been made towards the development of electrochemical methods for the detection of DNA sequences associated with human diseases and pathogens (Drummond *et al.* 2003; Ferapontova 2018), their application for plant pathogen detection has been relatively unexplored (Nezhad 2014; Fang and Ramasamy 2015; Khater *et al.* 2017; Ferapontova 2018). So far, only a few electrochemical DNA sensors for plant pathogen detection have been reported. However, most of these genosensors have certain limitations. For example, Wongkaew and Poosittisak (2014) reported a voltametric method for the detection of sugarcane white leaf (SCWL) disease. The method involved direct hybridisation of target organism genomic DNA with probes immobilised on chitosan-modified glassy carbon electrodes (GCEs) (Wongkaew and Poosittisak 2014). However, a high level of non-specific DNA binding to the electrode surface was observed on such platforms (Boriachek *et al.* 2018). Similarly, a highly sensitive method for the detection of the soilborne fungus *Trichoderma* involved complicated sensor fabrications (Siddiquee *et al.* 2014). On the other hand, a simple platform developed for the detection of *Citrus tristeza virus* (CTV) could achieve only a limited sensitivity (0.1  $\mu\text{M}$ ) (Khater *et al.* 2019). Signal amplification strategies based on redox reporters or chemical ligations sometimes lead to a loss of dynamic range (Qavi *et al.* 2010), which may be a crucial consideration in pathogen detection where a high degree of inter-sample variability in levels of target analyte/s is observed. Some of the other electrochemical methods of plant pathogen detection involve amplification of target DNA before electrochemical detection (Lau *et al.* 2017). Finally, almost all of the electrochemical methods reported so far rely on commercial kits or other complicated chemical DNA extraction procedures. These challenges are the major impediments to the development of platforms that can conduct on-farm pathogen testing and are simple enough to be used by semi-trained personnel such as farmers and extension workers.

In this study we sought to address several of these challenges. Specific aims of the study were to develop a leaf scald diagnostic method that: (i) is compatible with a simple one-step DNA isolation method; (ii) can provide naked eye/visual evaluation capability; and (iii) can provide amplification-free quantitative detection of *X. albilineans* DNA down to sensitivity levels suitable for routine diagnostics. We present a sandwich DNA hybridisation assay for colourimetric (naked eye) evaluation as well as electrochemical quantification of *X. albilineans* specific target DNA sequences in sugarcane sap.

## Materials and methods

### Reagents and materials

All reagents and chemicals used in this study were of analytical grade. Nuclease free distilled water (Invitrogen cat. no. 10977015; Thermo Fisher Scientific) was used for preparing all aqueous solutions. Screen printed gold electrodes

(SPGEs), DropSens DRP-220AT, were purchased from Metrohm DropSens (Spain). Mercaptohexanol (MCH), Tris (2-carboxyethyl) phosphine hydrochloride (TCEP), Tris-HCl, EDTA, 3,3',5,5'-tetramethylbenzidine (TMB), and phosphate buffered saline (PBS) tablets (0.01 M diphosphate buffer, 0.0027 M potassium chloride and 0.137 M sodium chloride; pH 7.4 at 25°C) were purchased from Sigma-Aldrich (Sydney). Horseradish peroxidase (HRP)-conjugated streptavidin (cat. no. SA10001) was purchased from Life Technologies Australia (Thermo Fisher Scientific). All synthetic probes and primers were purchased from Integrated DNA Technologies, Singapore. All electrochemical measurements were performed using a CH1040C potentiostat (CH Instruments, USA).

#### Sample collection and DNA isolation

Plants ~12 months old were inoculated with *X. albilineans* after 6 months of planting in the field. Sugarcane stalks were collected from the disease screening trial of SRA Woodford Research Station (26.929°E, 152.777°S), Woodford, Queensland, and immediately transported to the laboratory for extraction of xylem sap. Stalk samples were stored in clean plastic bags at 4°C until further analysis. Before extraction of DNA, stalks were cleaned thoroughly with Milli-Q ultrapure deionised water and 80% ethanol. Vascular sap was extracted from internode sections of stalks aseptically. Outer bark of stalks was shaved by using sterile scalpel blades. A new blade was used to cut the peeled internal tissue into small pieces (roughly 3–5 cm long, 1 cm thick), and the cut pieces of internal tissue were transferred to clean nuclease-free microcentrifuge tubes (1.5 mL). Disposable polypropylene pestles were used to extract sugarcane sap by applying pressure on the cut internal tissue pieces in the microcentrifuge tubes. To avoid cross contamination between samples, only one sample was processed at a time and fresh and sterile scalpel blades and pestles were used for each sample. Bacterial DNA was isolated from sugarcane xylem sap following the method reported by Garces *et al.* (2014). Briefly, collected sap samples (200 µL) were transferred to a clean microcentrifuge tube and centrifuged at 9000g for 5 min to precipitate bacterial cells. The pellet was resuspended in 100 µL lysis buffer (0.05 M KCl, 0.01 M Tris-HCl and 0.2% Tween-20; pH ~8.3) by vortexing vigorously followed by boiling at 95°C for 10 min. DNA from cultured *X. albilineans* was isolated using a DNeasy Plant Mini Kit (Qiagen). Isolated DNA samples were stored at –20°C until further use.

#### Capture and purification of target

Probes were designed targeting a 39-bp region (synthetic *XALB*; Supplementary Materials Table S1, available at the journal's website) within the albicidin pathotoxin biosynthesis gene cluster *XALB1* (GenBank accession no. AJ586576) (Royer *et al.* 2004). The target region was selected considering the pivotal role albicidin plays in leaf scald pathogenesis. The target region (synthetic target) corresponded to positions 1740266–1740304 in the *X. albilineans* GPE PC73 complete genome (GenBank accession no. FP565176.1) (Pieretti *et al.* 2009). Sequences

of the probes and synthetic target sequence are shown in Table S1. Known concentrations of synthetic target sequence were prepared by diluting stock solution (100 µM) in nuclease-free H<sub>2</sub>O. DNA purified from cultured bacteria was diluted to a concentration of 1 ng µL<sup>-1</sup>, whereas DNA from xylem sap samples was used without any further dilution. Each concentration was run in triplicate throughout (from target capture to detection).

The target sequences were separated and magnetically purified following our previously described protocol with slight modifications (Koo *et al.* 2016; Islam *et al.* 2018). Unless otherwise stated, all incubations in this section were performed for 30 min at room temperature and with shaking at 300 rpm. Briefly, a sample (10 µL), or nuclease free H<sub>2</sub>O<sub>2</sub> for no target control (NTC), was mixed with 15 µL 10 µM biotinylated capture probe 1 (CP1) and 10 µL 5× saline-sodium citrate (SSC) buffer (pH 4.0), heated at 95°C for 5 min, followed by cooling on ice and incubation. The required volume (10 µL sample<sup>-1</sup>) of Dynabeads MyOne Streptavidin C1 beads (Invitrogen) were washed three times with 1× binding and washing (B&W) buffer (10 mM Tris-HCl, pH 7.5; 1 mM EDTA, 2 M NaCl) and resuspended in 35 µL 2× B&W buffer. Washed beads were mixed with CP1-target mixture and incubated. The target-attached beads were magnetically separated, washed (two times with 1× B&W, once with 1× SSC buffer) and resuspended in 10 µL 5× SSC buffer. The captured target samples were stored at –20°C until further processing.

#### Sensor fabrication

Unless otherwise stated, electrodes were washed between each step using 10 mM PBS and dried by gentle air flow. The electrodes were protected from direct exposure to light throughout the experiments. The SPGEs were pre-treated electrochemically as described by Zhang *et al.* (2007). The effective area of working electrode was estimated by measuring the peak current obtained as a function of scan rate under cyclic voltammetric conditions for the one-electron reduction of [Fe(CN)<sub>6</sub>]<sup>3-</sup> (2.0 mM in PBS (0.5 M KCl)) (Shiddiky *et al.* 2009) and was determined by using the Randles–Sevcik equation:

$$i_p = (2.69 \times 10^5) n^{3/2} A D^{1/2} C \nu^{1/2} \quad (1)$$

where  $i_p$  is the peak current (A),  $n$  is the number of electrons transferred ( $\text{Fe}^{3+} \rightarrow \text{Fe}^{2+}$ ,  $n = 1$ ),  $A$  is the effective area of working electrode (cm<sup>2</sup>),  $D$  is the diffusion coefficient of [Fe(CN)<sub>6</sub>]<sup>3-</sup> (taken to be  $7.60 \times 10^{-5}$  cm<sup>2</sup> s<sup>-1</sup>),  $\nu$  is the scan rate (V s<sup>-1</sup>), and  $C$  is the concentration (mol cm<sup>-3</sup>).

Thiolated capture probes (CP2) were reduced by incubating 1 µL 1 mM TCEP with 99 µL 0.2 µM CP2. Equal volumes I-buffer (10 mM Tris-HCl + 1 mM EDTA + 0.1 M NaCl + 10 mM TCEP; pH 7.4) and reduced CP2 were mixed, and 5 µL of the mixture was placed onto the SPGE working electrode and incubated for 1 h. The working electrode was passivated with 5 µL MCH (1 mM) for 20 min.

The density of CP2 on the fabricated sensor was measured as described earlier (Wong and Gooding 2003; Shiddiky *et al.* 2010). Briefly, chronocoulometric (CC) measurements were

taken in 50  $\mu\text{L}$  E-Buffer (10 mM Tris-HCl; pH 7.0) and 50  $\mu\text{M}$  ruthenium hexamine,  $[\text{Ru}(\text{NH}_3)_6]^{3+}$ , (RuHex) by using following parameters: initial potential 0.2 V, final potential  $-0.5$  V, number of steps 1, pulse width 0.25 s, and sample interval 0.002 s. Charge ( $Q$ ) versus  $t^{1/2}$  for both CC runs was plotted and capacitive charge ( $Q_{\text{dl}}$ ) and total charge ( $Q_{\text{total}}$ ) were obtained from the intercept at  $t = 0$ , from the E-Buffer and RuHex plots, respectively (Supplementary Fig. S1). The charge corresponding to RuHex electrostatically bound to surface-confined ssDNA ( $Q_{\text{ss}}$ ) was calculated as described by Masud et al. (2017).

$$Q_{\text{ss}} = Q_{\text{total}} - Q_{\text{dl}} \quad (2)$$

The probe density ( $\Gamma_{\text{ss}}$ ) was calculated by using the following equation:

$$\Gamma_{\text{ss}} = \left( \frac{Q_{\text{ss}} N_A}{nFA} \right) \left( \frac{z}{m} \right) \quad (3)$$

where  $n$  is the number of electrons ( $n = 1$ ),  $A$  is the area of the working electrode,  $m$  is the number of nucleotides in the DNA,  $z$  is the charge of the redox molecules,  $F$  is Faraday constant, and  $N_A$  is Avogadro's number.

#### Colourimetric and electrochemical detection

Target solutions (10  $\mu\text{L}$ ) were added to the sensor surface for 1 h, followed by the incubation with 10  $\mu\text{L}$  biotinylated detection probe (DP) (10  $\mu\text{M}$ ) for 30 min and 4  $\mu\text{L}$  HRP-conjugated streptavidin (0.1 ng  $\mu\text{L}^{-1}$  in PBST) for another 20 min. The electrode was then incubated with 50  $\mu\text{L}$  TMB single solution (Invitrogen cat. no. 00-2023) for 10 min in the dark. Naked eye evaluation was done by observing blue colour development. The reaction was stopped by adding 4  $\mu\text{L}$  stop solution (0.2 M  $\text{H}_2\text{SO}_4$ ) to generate a yellow coloured complex. The amount of the enzymatically generated yellow coloured complex as an indicator of surface-bound target was measured by chronoamperometry at a fixed potential of +100 mV. All measurements were performed at room temperature.

#### Detection of leaf scald bacteria in samples collected from field trial

In order to demonstrate further the suitability of our method for field application, we analysed a series of sugarcane xylem sap samples. Samples were collected from nine cultivars of sugarcane from the SRA leaf scald screening trial. The trial was inoculated by manual decapitation of cane tops above the growing point, between the third and fourth dewlap, followed by application of infected juice within a few minutes, brushing the cut tissue with a paintbrush dipped in the inoculum. Sugarcane stalks were collected from nine cultivars (Q44, Q63, Q68, Q87, Q199, Q124, Q133, Q189, and Q208) in three categories of resistance to *X. albilineans* infection: susceptible, intermediate and resistant (three cultivars of each). For each cultivar, stalks from two different plants were collected initially (18 stalks in total). However, only 13 of the stalks were included in final analysis. The other five stalks were excluded mainly because of difficulties in obtaining a sufficient volume of sap for further analyses. Stalks of sugarcane cultivars were cut away from the nodes

into ~six pieces, each 12 cm, in order to extract xylem saps. Xylem sap was collected from three different segments of a single stalk as described above, and sap from each segment was processed independently. In total, sap samples extracted from 13 different plants corresponding to nine different cultivars were included in final analysis.

#### Validation with qPCR

A qPCR assay was designed with primers targeting a region of 123 bp from positions 1740257 to 1740379 in the *X. albilineans* GPE PC73 complete genome. The qPCR primers encompassed the whole synthetic target region (Table S1). qPCR validation was conducted in a CFX96 Touch Real-Time PCR Detection System (Bio-Rad Laboratories, Hercules, CA, USA) in a reaction (20  $\mu\text{L}$ ) using a SensiFAST Sybr No-ROX Kit (Meridian Bioscience, Cincinnati, OH, USA) and forward and reverse primers at a final concentration of 400 nM each (Table S1). The qPCR reaction conditions were as follows: initial denaturation at 95°C for 2 min; 40 cycles of 95°C for 5 s, 50°C for 30 s and 72°C for 20 s; followed by melt curve analysis (65°C to 95°C, with an increment of 0.5°C, for 5 s). Serial dilutions of known *X. albilineans* genomic DNA quantity (10 ng, 1 ng, 100 pg, 10 pg, 1 pg) were used to generate a standard curve for the absolute quantification of *X. albilineans* in sugarcane sap samples. For the validation and repeatability measurement, PROC CORR in SAS version 9.4 (SAS Institute, Cary, NC, USA) was used to calculate the correlations between electrochemical detection and qPCR measurements.

## Results and discussion

#### Assay design

The assay is schematically outlined in Fig. 1. Most of the DNA biosensing platforms reported so far rely on costly, time-consuming and tedious DNA extraction procedures. We adopted a simple boiling lysis-based method for bacterial DNA isolation directly from sugarcane xylem sap. Target DNA sequences (region of 39 bp within the *XALB1* gene cluster of *X. albilineans* genome) were specifically captured directly from this crude lysate by using complementary biotinylated probes (CP1) attached on the surface of streptavidin-coated magnetic beads. Subsequently, probe-bound target sequences were magnetically purified followed by heat release and magnetic purification. A self-assembled monolayer of thiolated CP2 on gold electrodes was prepared. CP2 are complementary to the target region adjacent to the CP1 complementary region. Surface density of the thiolated capture probes was in the range from  $1.2 \times 10^{12}$  to  $<5.0 \times 10^{12}$  molecules  $\text{cm}^{-2}$  in order to ensure efficient capture and sensitive detection of the target (see next section). The resultant target-CP2 hybrid on the gold electrode surface was reacted with biotinylated DP (CP1) to generate a sandwich CP2-DP:target assembly followed by binding of streptavidin-HRP to DNA assembly. HRP-catalysed TMB oxidation reaction yields a blue coloured product, which on the addition of concentrated acid is converted to a yellow coloured diimine compound. The intensity of the blue or

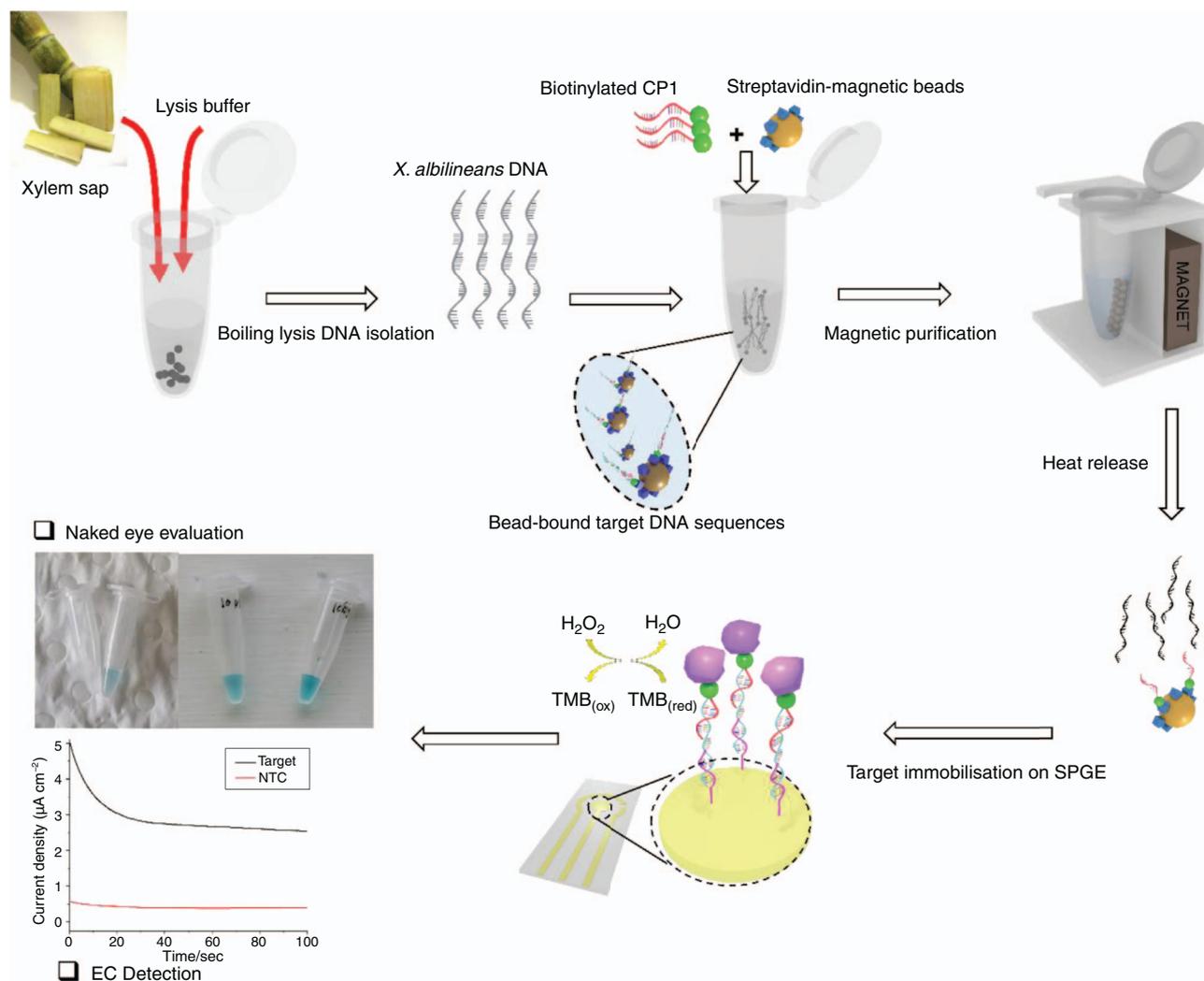


Fig. 1. Schematic representation of the assay for naked eye evaluation and electrochemical detection of *X. albilineans* DNA in sugarcane sap samples.

yellow coloured products provides an indirect measure of target concentration and was used for naked eye visualisation (blue colour) or electrochemical quantification via fixed potential chronoamperometry of the electroactive yellow coloured diimine compound (Fig. 1).

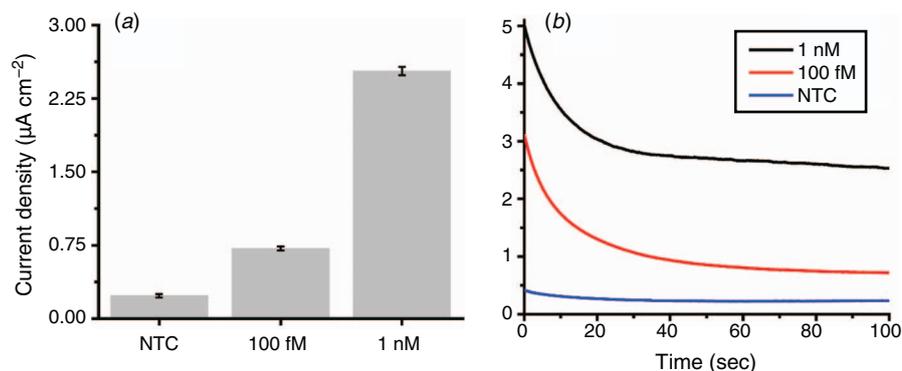
#### Determination of probe density

Performance of DNA-probe based sensors (e.g. selectivity, sensitivity and stability) is highly dependent on the characteristics of the immobilised DNA probes, such as conformation, orientation and surface density. The assembly of DNA probes at the sensor surface is affected by various parameters such as incubation time as well as concentration and ionic strength of immobilisation buffer (I buffer) as described by Zhang *et al.* (2007) and Shiddiky *et al.* (2010). The MCH used in these experiments not only serves as a spacer by finely modulating surface density of the DNA probes but also acts as a blocker that effectively blocks non-specific gold–DNA interactions on the electrode surface and helps DNA probes to ‘stand up’ on the electrode

surface, favouring the efficient hybridisation of incoming target sequences. DNA surface density was quantitatively measured by characterising the redox process of RuHex using CC readout. The electroactive label,  $[Ru(NH_3)_6]^{3+}$  (RuHex), is stoichiometrically bound to the anionic phosphate backbone of DNA strands via electrostatic interaction. RuHex complexes serve as signalling molecules whose cumulative redox charge is a direct function of the amount of DNA strand proximal to the electrode surface (Fig. S1). The probe densities obtained were in the range from  $1.4 \times 10^{12}$  to  $5.3 \times 10^{12}$  molecules  $cm^{-2}$ , which is within the range previously recommended ( $1.2 \times 10^{12}$  to  $<5 \times 10^{12}$  molecules  $cm^{-2}$ ; Zhang *et al.* 2007). For Fig. S1, the surface density of thiolated capture probes was calculated as  $5.3 \times 10^{12}$ .

#### Assay performance

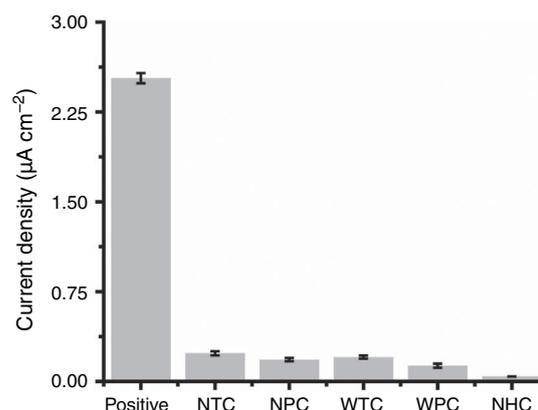
In order to demonstrate the viability of the assay, we compared the current response obtained in the presence of two designated synthetic target concentrations (1 nM and 100 fM) with that of



**Fig. 2.** (a) Current densities obtained for the analysis of known synthetic target concentrations (1 nM and 100 fM) compared with NTC (no target control, 1 nM). Error bars represent the relative standard deviation of three independent experiments (RSD <5%,  $n = 3$ ). (b) Corresponding representative amperograms for synthetic target detection.

NTC, which corresponds to a control reaction where nuclease-free water instead of synthetic target was mixed with CP1 functionalised beads, keeping all other assay components and subsequent steps consistent. As shown in Fig. 2a, an amperometric signal >10 times higher was obtained for 1 nM target DNA concentration than NTC (mean current density 2.5 vs 0.23  $\mu\text{A cm}^{-2}$ ;  $n = 3$ ). Similarly, low target concentration (100 fM) also showed significantly higher current response (0.71  $\mu\text{A cm}^{-2}$ ) than NTC (>3 times higher). Our assay design is based on 'sequential correlation' whereby the target concentration in the sample is directly correlated with the number of DNA molecules hybridised to the self-assembled monolayer of CP2 on SPGEs, which in turn is proportional to the concentration of biotinylated DPs confined to the target-CP2 hybrid. This way, the streptavidin-HRP concentration immobilised onto this sandwich DNA assembly and ultimately biocatalytic oxidation of TMB are directly proportional to the target concentration in the sample. Thus, current response obtained from the electrocatalysis of the yellow coloured diimine compound provides a direct measure of target concentration. Each concentration as well as NTC were analysed in triplicate, and intra-assay variability was evaluated by determining the percentage relative standard deviation (RSD) between the current responses obtained for each replicate. As indicated by error bars in Fig. 2a, our assay showed high repeatability, with RSD values of <5% obtained. Representative chronoamperograms obtained from the analysis of known target concentrations and NTC are shown in Fig. 2b.

High specificity of the signal is a prerequisite for electrochemical DNA assays. Several components of the assay may be able to contribute to background signal, including: interaction of probes with non-complementary sequences (a major concern when the starting sample is not a highly purified DNA but rather a crude lysate, which is essentially a heterogenous pool of various biomolecules such as proteins and RNA as well as sugarcane genomic DNA or DNA from any other microorganisms); non-specific adsorption of target and/or non-target DNA



**Fig. 3.** Current densities obtained for the control experiments compared with target (1 nM). Error bars represent the relative standard deviation of three independent experiments (RSD <5%,  $n = 3$ ). NTC, No target control; NPC, no probe control; WTC, wrong target control; WPC, wrong probe control; NHC, no HRP control.

sequences onto the bead surface; and nonspecific interaction of HRP with the gold electrodes. We systematically determined the possible effect of each assay component on the signal. As shown in Fig. 3 and Fig. S2, current response obtained for all controls was comparable with or less than NTC, thus indicating minimal interference from any of the assay components and highly specific target detection. In wrong probe control (WPC), non-complementary biotinylated and thiolated probes were used (sequences not shown), whereas in wrong target control (WTC), a synthetic DNA fragment corresponding to hsa-miR-891 was used, keeping all other components of the assay constant. Amperometric response obtained for both controls (mean current densities 0.13  $\mu\text{A cm}^{-2}$  for WPC and 0.20  $\mu\text{A cm}^{-2}$  for WTC;  $n = 3$ ) was similar to or less than NTC, indicating that the probes used in our assay are capable of capturing *X. albilineans* sequences with high specificity. No probe control (NPC) comprised 'mock purified' high target concentration (1 nM) where magnetic beads not

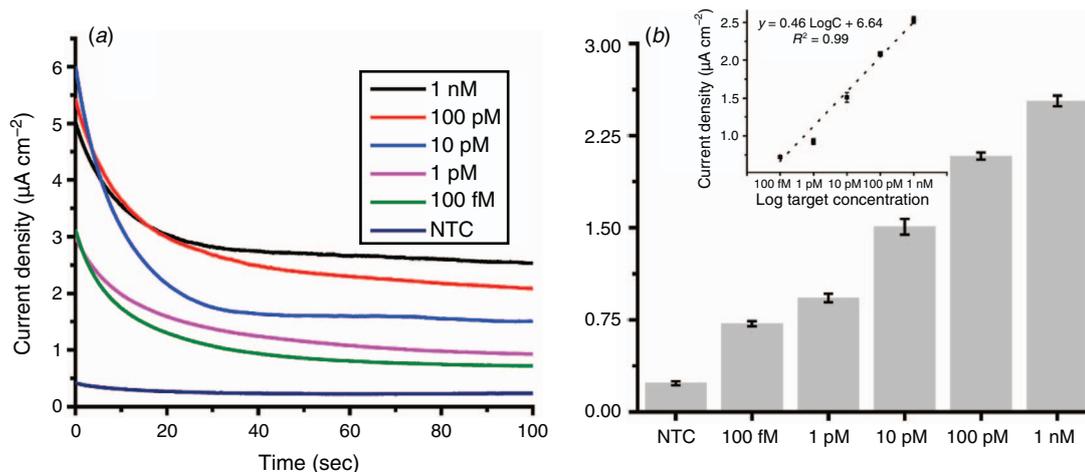
functionalised with biotinylated CP1 were mixed with target DNA. All subsequent assay steps remained unchanged. In no-HRP control (NHC), all assay steps were similar to the synthetic target reaction using a high concentration of target (1 nM), except at the stage of streptavidin–HRP immobilisation, where 0.1% PBST was introduced into the system rather than streptavidin–HRP. Mean current densities obtained for NPC and NHC were 0.18 and 0.042  $\mu\text{A cm}^{-2}$ , respectively. All control experiments were done in triplicate and showed high reproducibility (RSD <5%). Taken together, these results suggest high specificity of probes (WPC and WTC), low non-specific adsorption of DNA on beads or gold electrodes (NTC and NPC), and very little non-specific interaction of HRP with the sensor surface (compare NHC with other controls). Corresponding chronoamperograms for control experiments are given in Fig. S2.

A broad and linear dynamic range is an essential performance matrix for pathogen detection assays because high variability in target concentration is observed. Therefore, to assess the sensitivity and linearity of the assay, we analysed five different serially diluted concentrations of synthetic target DNA sequence (100 fM to 1 nM). As discussed previously, the electrochemical signal obtained in our assay is directly proportional to the analyte concentration. As shown in Fig. 4a, an increment in amperometric current response proportional to the increasing concentration of target DNA was observed. Our assay was able to detect synthetic target DNA reproducibly over a broad dynamic range between 100 fM and 1 nM. The linear regression equation was estimated to be  $y = 0.46 \log(\text{target concentration}) + 6.64$ , with a correlation coefficient of  $R^2 = 0.99$ , indicating good linearity of the assay (inset Fig. 4b). Limit of detection (LOD) of our assay, defined as the concentration of the analyte that can be reliably distinguished from NTC, was found to be 100 fM ( $S/n > 3$ ). All of the reactions were done in triplicate and RSD was calculated. RSD values for all samples were found to be <7%.

showing minimum intra-assay variability and excellent reproducibility. Our assay showed sensitivity 100 times better than one of the earlier reported sugarcane pathogen detection platforms, for which the authors reported a detection limit in the range of 10 pM (Wongkaew and Poosittisak 2014). On the other hand, a recently reported gold nanoparticle based plant virus detection platform could only achieve a lower detection limit of 100 nM; moreover, a logarithmic relationship was only observed within a very narrow range of concentrations (0.1–10  $\mu\text{M}$ ) (Khater *et al.* 2019). However, the platform reported by (Siddiquee *et al.* 2014) achieved attomolar-level sensitivity and detection over a very broad dynamic range ( $1.0 \times 10^{-18}$  to  $1.82 \times 10^{-4}$  mol L<sup>-1</sup>). Although this platform was several orders of magnitude more sensitive than our assay, it involved complicated sensor fabrication and relied on a tedious phenol-chloroform DNA extraction process (Siddiquee *et al.* 2014). By comparison, our assay provided a rapid, naked eye readout streamlined with a simple field-deployable DNA isolation method and without extensive sensor fabrication steps.

#### Detection of leaf scald in samples collected from field trial

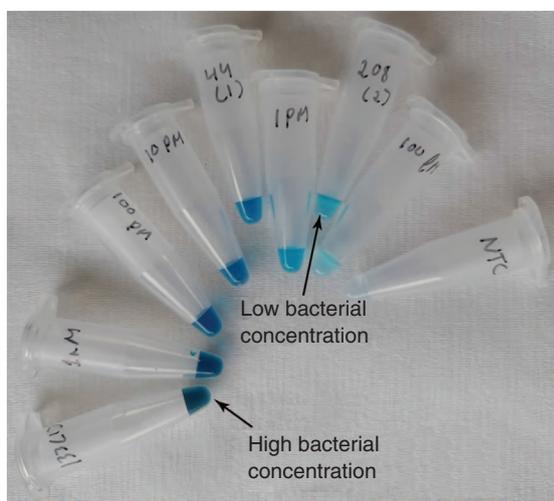
In order to further demonstrate the suitability of our method to real world applications, we analysed a series of sugarcane sap samples. Samples were collected from SRA Woodford leaf scald screening trial in an operator blind fashion. Samples were collected from varieties with various degrees of *X. albilineans* susceptibility (highly resistant to highly susceptible). The susceptibility/resistance status of the collected samples were known only to SRA staff. The Griffith team involved in conducting the electrochemical and molecular analyses were not aware of the sample susceptibility/resistance status during the method development stage. The target DNA was detected both colourimetrically (naked eye) and electrochemically. As shown in Fig. 5, development of blue colour was observed only in samples with known concentration of synthetic target



**Fig. 4.** Sensitivity and linearity of the biosensor. (a) The biosensor can reliably detect target DNA concentrations as low as 100 fM. Amperograms show distinguishable difference in current responses obtained for 100 fM and NTC. (b) The assay showed a linear response over a broad range of concentrations. Inset shows linear regression analysis of the data. Error bars represent the relative standard deviation of three independent experiments (RSD <7%,  $n = 3$ )

DNA or sugarcane sap samples, whereas NTC did not show any colour development. The intensity of the colour also provided a rapid qualitative result of bacterial concentration in the sample. Bright blue colour in sample 133 (1) (cultivar Q133) indicated high bacterial concentration, whereas sample 208 (2) (cultivar Q208) showed very low intensity suggesting low bacterial concentration in the sample (Fig. 5).

Target DNA was quantified electrochemically by performing chronoamperometric measurements as described earlier. As shown in Fig. 6a, the sensor successfully detected varying concentrations of target sequence in the samples collected from the field trial. The target DNA detected in most of the samples was within the LOD of our assay, indicating its applicability to real-world samples. In most of



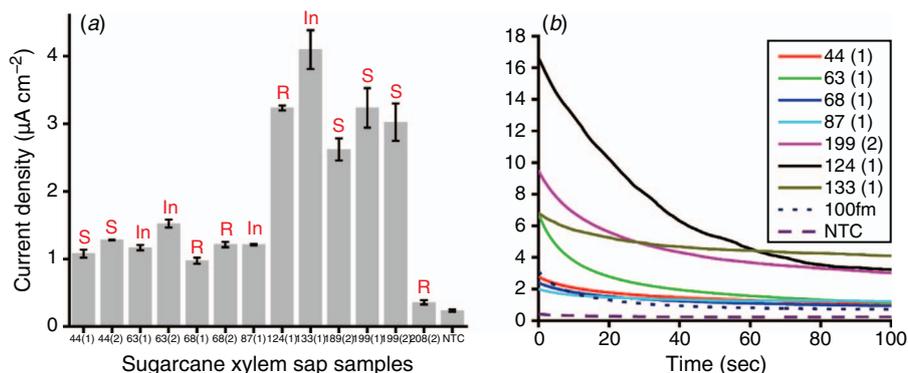
**Fig. 5.** Concentration-dependent increase in the intensity of TMB colour (blue) development (synthetic target DNA 100 fM–1nM). Representative photos for naked eye detection of *X. albilineans* DNA in sugarcane xylem sap; 133 (dark blue), 44 (moderate intensity) and 208 (light blue) indicate high, intermediate and low bacterial concentrations in sap samples, respectively.

the cases, detected *X. albilineans* DNA agreed with the resistance rating of cultivars. For example, a highly resistant variety such as Q208<sup>A</sup> (sample 208) consistently provided low response. However, some discrepancies between the expected bacterial concentrations and electrochemical response were also observed. For example, sample 44 (1), which was collected from susceptible cultivar (Q44), provided reduced current response. These discrepancies can be attributed to the age and the location of the stalks or where the samples were taken from. (Garces *et al.* 2014) reported variation of bacterial concentrations among types of tissues and plant ages. Nonetheless, all infected sugarcane samples collected were positive to the bacteria in our study. Figure 6b shows the amperograms for selected field trial samples.

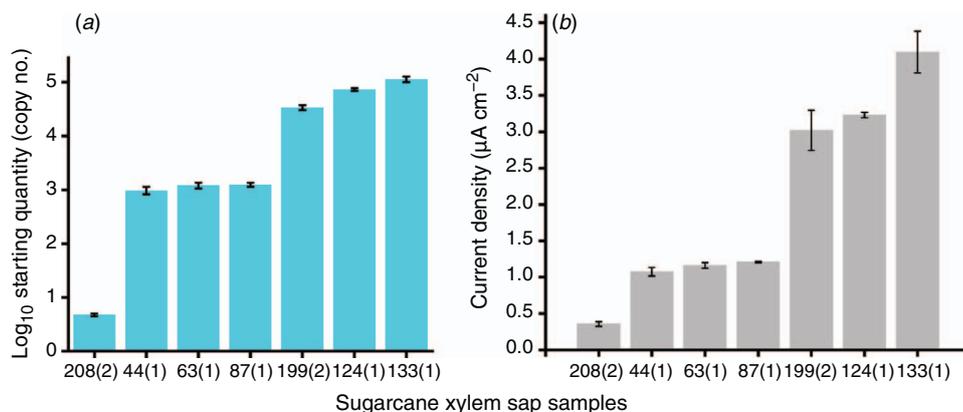
#### Validation of assay with qPCR

A qPCR assay was designed to validate the outcomes of our biosensor platform. The qPCR primers target a segment of 114 bp within the *XALB1* gene cluster (corresponding to positions 1740266–1740379 in *X. albilineans* GPE PC73 complete genome) that encompassed the region targeted in the electrochemical assay. The standard plot for qPCR-based absolute quantification was obtained by plotting C<sub>q</sub> (quantification cycle) values against log of corresponding known *X. albilineans* starting quantity. Absolute quantification of starting DNA copy number in field trial samples was calculated by comparing with the standard plot. The qPCR results depicted an excellent concordance with the electrochemical quantification, demonstrating that the newly developed biosensing assay is suitable for detecting *X. albilineans* in sugarcane sap samples (Fig. 7). The qPCR values were strongly correlated ( $r = 0.91$ ,  $P < 0.001$ ) with the biosensor assay (Table 1). The strong correlation ( $r = 0.99$ ,  $P < 0.0001$ ) of C<sub>q</sub> value of biosensor and qPCR samples showed repeatability of the test.

In this proof-of-concept study, we have demonstrated sensitive (up to femtomolar level) detection of the



**Fig. 6.** (a) Current density bar graphs for all the analysed samples from SRA Woodford leaf scald screening trials (xylem sap extracted bacterial DNA). Error bars represent the relative standard deviation of three independent experiments. Data labels represent resistance rating: S, susceptible; In, intermediate; R, resistant. Note: discrepancies between the expected bacterial concentrations (based on resistance rating) and current response are discussed in the text (*Results and discussion*). (b) Amperograms for a selected set of samples.



**Fig. 7.** Validation of the biosensor data using qPCR: (a) starting quantity (copy number) for a selected set of samples as determined by qPCR based absolute target quantification; (b) current density obtained for the corresponding sugarcane xylem sap samples. Error bars represent the RSD of three independent experiments.

**Table 1.** Pearson correlation coefficients to compare relationship of current density ( $\mu\text{A cm}^{-2}$ ) from the samples collected from the field trial and qPCR validation samples

$^{**}P \leq 0.001$ ;  $^{***}P \leq 0.0001$

Parameter	Log starting quantity (qPCR sample)	Current density (qPCR sample)
Current density (field trial sample)	0.91 <sup>**</sup>	0.99 <sup>***</sup>
<i>N</i>	7	7
Log starting quantity (qPCR sample)		0.89 <sup>**</sup>
<i>N</i>		7

sugarcane pathogen *X. albilineans* in xylem sap samples. The assay offers some significant advantages. First, we have demonstrated that our assay is compatible with the boiling lysis-based DNA extraction method. When compared with kit-based or organic extraction-based DNA isolation methods, the boiling lysis method is not only low-cost, but also potentially field deployable because it requires relatively simple instruments (centrifuge, heat block). Also, crude lysate is a more stable sample source and more resistant to degradation and contamination than cut stalks. Thus, instead of shipping sugarcane stalks, the bacterial DNA can be extracted by using a simple on-farm setup and sent to remote laboratories for testing. In the case of colourimetric detection, the process takes <1 h and gives a first pass yes/no answer. Electrochemical assay utilises disposable screen-printed electrodes, which cost as little as ~US\$3 each, making overall per sample cost of the assay <\$10. Finally, unlike most of the electrochemical assays reported previously, our method achieves sensitive target detection without complicated sensor fabrication steps.

This generic technology is flexible in the sense that it is potentially applicable to almost all types of pathogens by using specific probes. Our assay could be applicable for the diagnosis and management of diseases in other agricultural and horticultural crops, and potentially in other environments (e.g. in soil). Moreover, using multi-well screen-printed electrodes, the platform can be further extended for high throughput and/or multiplex detection of various pathogens

simultaneously. The assay could also form the basis of a fully integrated, next-generation handheld device, associated with a purpose-built smartphone application. Such a device can be particularly useful in developing geographic information systems (GIS) for surveillance as well as prevalence and risk mapping of various diseases. The proposed integrated device can also be used for developing rapid screening and warning systems for exotic diseases to be implemented at entry points like airports and seaports.

### Conclusion

We have developed a sensitive method for the detection of leaf scald disease of sugarcane. This method offers a dual detection where naked eye evaluation of colour change provides qualitative detection of *X. albilineans*, and quantification up to femtomolar levels of target DNA was achieved by electrochemistry. Our assay showed high specificity, good linear response ( $R^2 = 0.99$ ) for detection of target concentrations 100 fM–1 nM, and excellent repeatability (RSD <7%,  $n = 3$ ). The proposed assay can potentially be used for detection of a range of sugarcane and other agricultural pathogens and can also form the basis of next generation portable integrated devices for on-farm applications.

### Conflicts of interest

The authors declare no competing financial interest.

### Author contributions

MU and NBA equally contributed to this work.

### Funding statement

This work was jointly supported by SRA through Innovation Catalyst Project (INNOVA 06) and Griffith University ESC Research Support Scheme 2018.

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Handling Editor: Angela Van de Wouw